Amendments to the Specification:

On page 1, after the title and before line 1, please insert the subheading:

BACKGROUND

On page 1, please amend the first paragraph spanning lines 1-5 to read as follows:

The invention relates to a magnetic resonance method for forming a fast dynamic image form a plurality of signals of an RF probe according to the preamble of claim 1. The invention further relates to a magnetic resonance imaging apparatus for obtaining a fast dynamic image according to the preamble of claim 11 and to a computer program product according to the preamble of claim 12.

On page 2, please amend the fourth paragraph spanning lines 14-16 to read as follows:

This and other objects of the invention are accomplished by a method as defined in claim-1, by an apparatus as defined in claim-6 and by a computer program product as defined in claim-7.

On page 2, after line 21 and before line 24, please insert the subheading:

BRIEF DESCRIPTION OF THE DRAWINGS

On page 2, line 24 through page 3, line 11, please amend that section to read as follows:

Fig. 1 a Figs. 1a-1c are schematic view views of a patient at three different positions moved through the bore of a main magnet for MR imaging,

Fig. 2 Figs 2a-2c illustrate the data for each table position of Fig. 1,

Fig. 3 illustrates the virtual sensitivity map for the full FOV,

Fig. 4 is a schematic representation of the final image and FOV after reconstruction,

Fig. 5 Figs 5a-5c illustrate an arrangement with a separate array of body coils mounted on the patient table,

Fig. 6 <u>is illustrative of prior</u> art imaging showing data from two separated stations of the phantom and the combination of both data sets,

Fig. 7 <u>illustrates</u> prior art imaging showing data measured by the same stations as in Fig. 6 with a band limiting filter in the measurement (frequency encoding) direction,

Fig. 8 Figs 8a-8c illustrate a first embodiment according to the present invention showing a phantom scanned at 3 different positions moved through the bore of the main magnet of an MR imaging system,

Fig. 9 <u>illustrates</u> a second embodiment according to the present invention, wherein data is measured as in Fig. 6 with a SENSE factor of 1.33 at each station,

Fig. 10 <u>illustrates</u> the different steps for decoding the data according to the present invention, and

Fig. 11 <u>illustrates</u> a third embodiment according to the present invention, wherein data is measured at three separate stations, with different SENSE factors and its reconstruction.

On page 3, after line 11 and before line 14, please insert the subheading:

DETAILED DESCRIPTION

On page 4, please amend the second full paragraph spanning lines 12-30 to read as follows:

In figure 1 figures 1a-e, the contours of a main magnet 1 with a magnet bore 2 is schematically depicted. A patient 3 on a movable table 4 can be moved through the bore 2 in discrete steps, here at three different table positions in which the abdomen of the patient is scanned (Fig. 1a), the breast of the patient is scanned (Fig.

1b) and the head of the patient is scanned (Fig. 1c). Within the main magnet 1 there are mounted a transmitting quadrature body coil 6 and a smaller receiving quadrature body coil 7. The receiving coil 7 is defining the dimensions of the Field-of-View (FOV) of the image. In this example data with the restricted FOV 8 of the receiving coil 7 are sampled, in order to form a single MR-image of the entire region of interest or full FOV 9 as indicated by the dashed lines. Arrow 10 indicates the encoding and/or foldover direction. The subsequent data sampled at the three table positions are reconstructed by the SENSE method. In figure 2 figures 2a-c, the images at each table position encoded for the full FOV 9 is are shown, whereas different fold-over artefacts are obtained from each different scan. In figure 3 the virtual coil sensitivity map for each of the table positions are shown, which is actually a triplicate of the single sensitivity map of the single receiving coil 7. From the sensitivity map of the full FOV (Fig. 3) an unfolded image can be reconstructed as shown in a schematic representation of the final image and the full FOV. The total number of encodings acquired is just the same as if a fully encoded scan would be possible on the full FOV, here 3 * N pixels as N encodings are provided for the restricted FOV.

On page 5, please amend the first full paragraph spanning lines 1-6 to read as follows:

Another embodiment of the present invention is shown in figure 5 figures 5a-c in which an array of local surface coils 11 are mounted at a fixed position relative to the patient 3, i.e. relative to the table 4. Thus, these coils 11 are moved by the table movement and only the ones which are positioned within the restricted FOV of the transmitting coil 6 are activated to receive the transmitted RF signals. In this case the sensitivity maps of the coils 11 are needed to reconstruct the final image by the SENSE method.

On page 7, after the last paragraph ending on line 31, please insert the following new paragraph:

The invention has been described with reference to the preferred embodiments. Modifications and alterations may occur to others upon reading and understanding the preceding detailed description. It is intended that the invention be construed as including all such modifications and alterations insofar as they come within the scope of the appended claims or the equivalents thereof.